Amendment to the Specification:

Please replace the paragraph starting at Page 7 line 3 with the following:

Figure 2 is a view of a stent graft system of Figure 1, in which the stent graft has been deployed. The syringe plunger has been depressed so as to force fluid from the syringe into the catheter and into a fluid delivery chamber (described in detail below). Such an introduction of fluid, under sufficient pressure, causes the containment sheath 52 to move proximally, in proximal direction shown by the arrow 64, so as to ultimately abut against backstop 50. This movement causes the lumen of the containment sheath 52 to no longer contain a stent graft 60 formerly contained therein. The containment sheath 52 is moved to a location equal to or beyond the stent cup plunger 66. Stent cup plunger 66 is a ring type structure engaged with the catheter body 34 and is sized to snugly fit within the containment sheath 52 wherein the stent cup plunger 52 acts as the end surface of the anti kink spacer which as the spacer coils are compressed and contact one another and become inflexible establishes a limit for the movement in the proximal direction by the stent graft 60 as the containment sheath 52 is moved in the proximal direction 64.

Please replace the paragraph starting at Page 12 line 5 with the following:

Figure 9A and 9B show the partial cross section of two alternative constructions of a containment sheath according to the invention. A first material section [[96]] 98 having friction reducing qualities (such as PEBAX) for the easy release of a spring loaded (self expanding) stent graft contained therein is fixed through a fused joint 95 to a second more rigid material section [[98]] 96 whose material qualities are chosen to maintain rigidity (e.g., PE) and the sealing of the fluid receiving chamber 75. In the configuration of Figure [[9b]] 9B, similarly a first material section 97 has increased lubricity on its inner surface, while a second material section 99 has structural properties compatible with use as walls of pressurized chambers and for maintaining seal integrity. The change in diameters shown in Figure 9B is done through a transition section 101 with a joint 100 between the two material section, though the transition section could be a third material. In the construction of this configuration a standard sized catheter could be used all the way to the location of the joint, before the transition to a larger size is attached, reducing the need for specialized structures. Further as shown the thickness of the two section can be varied according the structural requirements, e.g., the stent containing portion 97 has a thinner wall than the second material retraction section 99.